

Beside for
intercellular route
(cevc 2004, tang et



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Beside SC, tight junction proteins (claudin, occluding and zonulaoccludins-1) have been implicated for providing barrier function to skin . Otherthan barrier like property of skin outside, there are many factors which affectthe delivery of the drug and they are discussed in the following

section. FACTORS AFFECTING NANO BASEDTRANSDERMAL DRUG

DELIVERYSYSTEM

PARTICLE SIZE and ShapeThe nanodrugs

transdermal delivery is affected by its size and shape which further decide physical steadinessand their cellular uptake (Escobar Chavez et al 2012).

Nanoformulations can bedelivered concurrently using different means/routes owing to their particlesize and physicochemical properties (Borali 2010). Skin anatomical featuresonly allows free distribution of particles <5-7 nm size throughtranscellular route (Bouwstra and Ponec 2006, Johnson et al 1997), ? 36 nm forintercellular route (Cevc 2004, tang etal. 2001) and > 3-10 μm for transfollicular route.

Particles of smaller sizeare preferred since they make available larger surface area hence can have highdrug loading capacity. Attama et al (2007) reported that low particle size solid lipidnanodispersions (SLN) aremore stable and well accepted in vivo and active formulkation had high drugconcentration. Maestrelli et al (2009), who investigated ethosomes prepared by differenttechniques made similar conclusions and found that small unilamellar vesicles(SUVs) drug efficacy of benzocaine (BZC) was owing to its small size, highersurface area which led to more intimate contact with the epithelium for longerduration of time for therapeutic action.

Desaiet al. (2010) and Baroli (2010) concluded that lipophilic nanoparticles havehigh partition coefficient and drugs having molecular weight <600 Da

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are best suited for TDDS. Nanoparticles come in different shapes like spherical, ellipsoidal, triangular, needle shaped, cubic and prism like. They are not always rigid (e.

g. lipid particles) and deformable. The shape as well as orientation of the nanoparticles greatly affects their aggregation, penetration route and diffusion coefficient (Baroli 2010).

Using newer methods of nanomaterial synthesis, nanoparticles of preferred size and shape for TDDS can be engineered. ZETA POTENTIAL Zeta potential is defined as the number of charges a particle has and particle size distribution and zeta potential of nanoformulations decides the dispersion steadiness of the non-aqueous suspension. SIZE DISTRIBUTION Preparation methods and conditions (like temperature, dispersing medium, stirring rate and viscosity of the organic and aqueous phases) affect the size distribution of nanoparticles formed by different systems. Skin SURFACE

PROPERTIES Surface properties of the skin like surface charge and polarity are also key determinants for drug penetration profile in TDDS. Charges on the skin surface generally influence the ionic interaction of drug molecules with cell membrane, route of penetration and diffusion rate in vivo. Surface charge of the cell membrane is due to presence of negatively charged phosphatidyl choline and sulphated proteoglycans. They are membrane anchored core proteins which are linked to glycosaminoglycan side chains (heparan, dermatan, keratan or chondrotine sulfates) that protrude from the cell surface.

Due to this negative charge in skin at neutral pH, positively charged nano formulations diffuse effectively through skin. Hoeller et al. (2009) reported

effective permeation of drug through porcine skin using phytosphingosine (PS) containing positive charged nanoemulsion than the negatively charged ones. Generally negatively charged nanoparticles are repelled by cellular membrane, however they are absorbed by non specific process of nanoparticle cluster formation at positive charged sites which lead to neutralization followed by cellular uptake by the process of endocytosis